Transurethral Anastomosis after Transurethral Radical Prostatectomy: A Phantom Study on Intraluminal Suturing With Concentric Tube Robots

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Abstract—Current surgical approaches to radical prostatectomy are associated with high rates of erectile dysfunction and incontinence. These complications occur secondary to the disruption of surrounding healthy tissue, which is required to expose the prostate. The urethra offers the least invasive access to the prostate, and feasibility has been demonstrated of enucleating the prostate with an endoscope using Holmium laser, which can itself be aimed by concentric tube robots. However, the transurethral approach to radical prostatectomy has thus far been limited by the lack of a suitable means to perform an anastomosis of the urethra to the bladder after prostate removal. Only a few intraluminal anastomotic devices currently exist, and none are small enough to pass through the urethra. In this paper we describe a new way to perform an anastomosis in the small luminal space of the urethra, harnessing the dexterity and customizability of concentric tube manipulators. We demonstrate a successful initial proof-of-concept anastomosis in an anthropomorphic phantom of the urethra and bladder.

Index Terms—Transurethral Suturing, Concentric Tube Robots, Minimally-Invasive Surgery, Natural Orifice Surgery

I. INTRODUCTION

Prostate cancer is the most prevalent cancer in men. In every 9 men will develop prostate cancer in their lifetime, with over 190,000 new diagnoses per year in the USA alone [1]. Many of these patients will undergo radical prostatectomy, which is often performed using the da Vinci robot through the abdomen. Transabdominal radical prostatectomy requires mobilizing the prostate via extensive dissection/retraction of surrounding anatomical support structures, nerves, and blood vessels. After prostate removal, an anastomosis is performed to re-connect the urethra to the bladder, a task where the da Vinci’s wrist dexterity and stereo vision capabilities are particularly useful. Complications including incontinence and erectile dysfunction are known to occur following surgery, and have been reported to be as high as 70% for erectile dysfunction and 21% for urinary incontinence [2]. Although outcomes related to specific hospitals and specific surgeons vary widely, some level of these complications is intrinsic to the procedure as currently performed.

It is generally agreed by surgeons that the required dissection and retraction of nerves and other structures is largely responsible for these complications. The goal of minimizing this disruption of surrounding structures has motivated exploration of transurethral approaches, which have been attempted with straight, rigid endoscopes [3]–[5]. In these procedures, the prostate is removed with a fiber optic laser delivered through an endoscope, a procedure that is similar to Holmium Laser Enucleation of the Prostate, with the additional removal of the prostate capsule. The main conclusion of these studies was that resection was possible with standard techniques, but that more dexterous tools at the endoscope tip are needed, to enable high-quality anastomotic suturing [3], [6], [7]. In this paper, we propose the use of needle-size, precurved concentric tube manipulators [8], [9] delivered through an endoscope to...
enable anastomotic suturing after radical prostatectomy. The feasibility of tissue removal with such a system [10], as well as tendon-based sheaths [11] has been shown in the context of transurethral enucleation for benign prostatic hyperplasia (BPH), and similar systems have been used in neurosurgery applications [12], [15]. However, the reconstruction of the bladder to the urethra after prostate removal remains a fundamental challenge. In this work, we demonstrate the feasibility of performing a transurethral anastomosis on a urethra-bladder phantom, using two concentric tube manipulators to perform suturing.

II. MATERIAL AND METHODS

Our suturing approach uses two concentric tube manipulators delivered through a rigid endoscope. The needle arm (the left arm in Fig. 1) pierces tissue in Fig. 1A, grasps the suture in an end effector conceptually similar to a kidney stone retrieval basket (Fig. 1B), and then pulls the suture through tissue (Fig. 1C). The other concentric tube arm, which functions as a grasper with a forceps at its tip, then manipulates the suture back into the bladder in preparation for the needle arm’s next pass (Fig. 1D). The result of several such sutures is a complete anastomosis as shown in Fig. 1E.

A. Concentric Tube Manipulator and Needle

The tube parameters summarized in Fig. 2, top describe the manipulator arm (top) and needle arm (bottom). The needle arm consists of one curved tube with the curvature of $\kappa_N = 20 \text{ m}^{-1}$ and curved section length of $L_{c,N} = 50 \text{ mm}$. The tube tip is manually ground into a beveled point, so that it can easily pierce tissue. To grasp suture, a modified kidney stone retrieval basket is deployed through the needle arm (Zero Tip™, Boston Scientific, Marlborough, MA, USA). The cross-section of the needle tube is elliptic to lock the axial rotation [13], which prevents elastic instability while enabling follow-the-leader insertion [14] in which the needle shaft follows its tip exactly.

The manipulator arm consists of two tubes. The outer tube is straight and inner is curved with tube curvature $\kappa_M = 25 \text{ m}^{-1}$ and curved length of $L_{c,M} = 25 \text{ mm}$. The forceps fixed at the tip of the inner tube was adapted from the 27023 FE Grasping Forceps (Karl Storz, Tuttingen, Germany). Fig 2, bottom right shows the prototype of the concentric tube arms deployed through the endoscope. A 26 Fr resectoscope (27050 SC) with a wide angle lens (27292 AMA Hopkins® , Karl Storz, Tuttingen, Germany) nested inside an aluminum sheath was used to access the surgical site transurethrally (Fig. 3, bottom left). The lens has a 6° angled view downwards.

Three customized stainless steel guide tubes were delivered through the 5 mm channel in the resectoscope. Two of them were made with an elliptic cross-section and enable delivery of the needle arm (only one of these oval guides was used at a time for the needle arm). The elliptic cross-section guide tubes point away from the centerline helping to aim the needle arm toward the urethral wall. The third guide tube (in the center) has a round cross-section and facilitates insertion of the manipulator arm. All three guide tubes are glued at the tip of the aluminum sheath via a customized 3D-printed adaptor.
B. Experimental Setup

We demonstrated our transurethral anastomosis concept in an anatomical phantom model consisting of a silicone bladder and urethra (Shore A30), mounted on rubber bands and foam (see Fig. 4 right). The bladder neck diameter is 14 mm and the wall thickness is approximately 2.5 mm. These anatomical dimensions were extracted manually from pelvic MRI images. The urethral inner diameter was set to 12 mm, which is slightly larger than a human urethra, in order to accommodate our aluminum outer sheath, which has an inside diameter comparable to a clinical sheath, but a larger (12.5mm) outside diameter. We note that the aluminum outer sheath was used simply for convenience in this work and will be replaced in the near future with a stainless steel sheath that matches clinical equipment dimensions exactly. The fact that our experiments were successful through an accurate inside diameter provides an indication that this replacement should be straightforward. To improve visualization of the manipulators during suturing, we added a translational degree of freedom for the resectoscope lens, enabling it to linearly extend from the tip of the outer sheath (see Fig. 4, right). The translation of the lens in our system was performed manually by sliding the lens forward within a 3D-printed housing as shown in Fig. 4, right (orange arrow). The robot arms are moved by a motorized actuation unit based on the differential drive mechanism of Rox et al. [15] providing 2 DoF for each concentric tube, enabling translation and rotation. This actuation unit was used previously by Gafford et al. for bronchoscopy in the central airway [16]. The actuation unit was mounted in a ball bearing frame providing manual (i.e. non-motorized) pitch, roll, and yaw, and additional translation of the whole actuation unit along the endoscope axis. The setup is shown in Fig. 4.

C. Experimental Evaluation

We investigated the feasibility of our proposed suturing approach using the phantom and the prototype described previously. The bladder and the urethra were separated by approximately 25 mm, representing the surgeon operator’s estimate of the anatomical configuration during surgery after the prostate removal and immediately prior to anastomosis. A urologic surgeon used a graphical user interface to move the tubes in the concentric tube robot, and an assistant positioned the robot itself and actuated the end effectors based on instructions from the surgeon. Only visual feedback from the endoscope was used to perform the experiments. Several prior initial anastomosis were performed to discover potential challenges and experiment with different suturing approaches. Two barbed sutures, each 100 mm long, (Stratafix Symmetric PDS 3-0, Ethicon, Bridgewater, NJ, USA) were used. The suture has an anchor on one end, with uni-directional barbs that prevent it from sliding backward through tissue, without the need to tie knots. This suture was placed in the bladder manually. The forceps was used to grasp and hold the bladder wall to stabilize it and facilitate needle passage (Fig. 5A). The forceps was then used to manipulate the suture and place it inside the basket (Fig. 5B1-B2). After the suture was pulled through the bladder and then urethra wall by the needle arm (Fig. 5C), the forceps was used to move it inside the urethra and back into the bladder in preparation for grasping after the next needle pass (Fig. 5D). To evenly distribute the suture circumferentially, the actuation unit was rotated inside the bearing frame (i.e. about the endoscope axis) and the needle arm was switched between the two elliptical guide tubes as needed.

III. Results

The anastomosis was performed with 7 stitches using two running sutures and one interrupted suture. As shown in Fig. 5E,II, the urethra and bladder were successfully anastomosed. Sutures were first started at antipodal points to fix the radial orientation of the bladder and urethra to each other. Afterwards, the suture was alternated following every 2 needle passes to ensure even circumferential suture spacing and prevent anastomotic gaps. Tightening the sutures occurred after placement of the final stitches, to minimize individual suture tension and enable the endoscope to view the space outside the urethra during needle passes, as needed. The single interrupted suture was placed to close a residual gap in the anastomosis left by the two running sutures at the 12 o’clock position, as is conventionally performed from outside.
the anastomosis for remaining gaps in da Vinci-assisted radical prostatectomy. Such a gap is typically the result of the opening of the anastomosis for remaining gaps in da Vinci-assisted radical prostatectomy for leaks. If these experiments are successful, the system will provide exactly the type of new and improved instrumentation with enhanced dexterity that has limited clinical deployment of transurethral radical prostatectomy in the past. More broadly, our new suturing approach provides a means of performing suturing at the tip of a thin endoscope, enabling suturing in much more highly constrained areas of the body than has previously been possible.

IV. CONCLUSION

This paper proposes a new approach to suturing within a lumen using transendoscopic concentric tube manipulators, and demonstrates its feasibility in a phantom model. Novel features of our system include a new axial endoscope lens degree of freedom, and the use of specialized needle and manipulator arms. The needle arm uses ellipsoidal cross-sections to enable follow-the-leader deployment, and the manipulator arm features round cross-sections for more general movements. In future work, we plan to perform suturing studies comparable to those described in this paper in a cadaver model. We note that the current work is simply an initial feasibility study on a new concept for passing sutures to perform anastomosis from within the lumen. Future work is needed to address repeatability, time efficiency, and test the resulting suture lines for leaks. If these experiments are successful, the system will provide exactly the type of new and improved instrumentation with enhanced dexterity that has limited clinical deployment of transurethral radical prostatectomy in the past. More broadly, our new suturing approach provides a means of performing suturing at the tip of a thin endoscope, enabling suturing in much more highly constrained areas of the body than has previously been possible.

REFERENCES